



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶ : A61B 17/00	A2	(11) International Publication Number: WO 98/55027 (43) International Publication Date: 10 December 1998 (10.12.98)
<p>(21) International Application Number: PCT/US98/09187</p> <p>(22) International Filing Date: 5 May 1998 (05.05.98)</p> <p>(30) Priority Data: 08/669,808 5 June 1997 (05.06.97) US</p> <p>(71) Applicant: VASCULAR SCIENCE INC. [US/US]; Suite 202, 701 Decatur Avenue North, Minneapolis, MN 55427 (US).</p> <p>(72) Inventors: SULLIVAN, Daniel, J.; 1245 Oak View Road, Medina, MN 55356 (US). GOLDSTEEN, David, S.; 4885 East Lake Harriet Parkway, Minneapolis, MN 55409 (US).</p> <p>(74) Agents: JACKSON, Robert, R. et al.; Fish & Neave, 1251 Avenue of the Americas, New York, NY 10020 (US).</p>		<p>(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, GH, GM, GW, HU, ID, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, UZ, VN, YU, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).</p> <p>Published <i>Without international search report and to be republished upon receipt of that report.</i></p>
<p>(54) Title: MINIMALLY INVASIVE MEDICAL BYPASS METHODS AND APPARATUS USING PARTIAL RELOCATION OF TUBULAR BODY CONDUIT</p> <p>(57) Abstract</p> <p>A tubular body conduit can be partly relocated intraluminally (e.g., to provide a bypass around a narrowing of a tubular body conduit). The tubular body conduit may be plugged intraluminally beyond the part to be relocated. Then the conduit is cut intraluminally. The severed portion of the conduit is relocated intraluminally (e.g., to place the severed end adjacent the side wall of another conduit). The side wall of the other conduit is penetrated intraluminally and the two conduits are connected by a connector that is installed intraluminally.</p>		

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**MINIMALLY INVASIVE MEDICAL BYPASS
METHODS AND APPARATUS USING PARTIAL
RELOCATION OF TUBULAR BODY CONDUIT**

Background of the Invention

5 This invention relates to methods and apparatus for treating medical patients who are in need of re-routed body conduits. An example of the use of this invention is in the partial re-routing of a patient's internal mammary artery to provide a bypass around a blockage or constriction in a coronary artery of the patient.

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A well-known technique for relieving the adverse effects of a coronary artery blockage or constriction is to sever one of the patient's internal mammary arteries and reconnect the portion of that artery which comes from the aorta to the blocked or constricted coronary artery downstream from the blockage or constriction. The thus re-routed mammary artery supplies the blood flow needed in the downstream portion of the coronary artery.

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A disadvantage of known procedures for re-routing an internal mammary artery is that these procedures require either a large opening of the patient's chest cavity or several small openings in that cavity.

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In view of the foregoing it is an object of this invention to provide methods and apparatus for reducing the degree of invasiveness of medical treatments involving the partial relocation of a 5 patient's tubular body conduit such as in the relocation of a portion of the patient's internal mammary artery to provide a cardiac bypass connection.

Summary of the Invention

This and other objects of the invention are 10 accomplished in accordance with the principles of the invention by providing methods and apparatus for intralumenally (or at least partly intralumenally) partially relocating a portion of a patient's tubular body conduit. In accordance with the invention, the 15 location at which the patient's tubular body conduit is to be severed is approached intralumenally. A plug may be deposited in the conduit downstream from the point at which the conduit is to be severed. The conduit is then severed from inside its lumen. Any connective 20 tissue between the portion of the conduit that is to be re-routed and surrounding body structures is severed, either by instrumentation which emerges from the severed end of the conduit or which is introduced via a separate opening made into the patient. The portion of 25 the conduit to be re-routed is then intralumenally relocated so that its severed end is adjacent the desired new point of attachment of the severed end. A connector structure attached intralumenally to the severed end of the relocated conduit is then used to 30 form an aperture in the side wall of the other conduit to which the relocated conduit is to be connected. After making this aperture, the connector structure

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connects the severed end of the relocated conduit to the aperture in the other conduit.

Further features of the invention, its nature and various advantages will be more apparent from the 5 accompanying drawings and the following detailed description of the preferred embodiments.

Brief Description of the Drawings

FIG. 1 is a simplified sectional view of a portion of a patient's circulatory system.

10 FIG. 2 is a view similar to a portion of FIG. 1 showing an early stage in an illustrative use of the invention.

15 FIG. 3 is a view similar to FIG. 2 showing a later stage in the illustrative use of the invention that is shown in part in FIG. 2.

FIG. 4 is a view similar to FIG. 3 showing a still later stage in the illustrative use of the invention that is shown in part in FIG. 3.

20 FIG. 5 is a view similar to a portion of FIG. 4 showing an alternative to FIG. 4 in accordance with the invention.

FIG. 6 is a view similar to FIG. 4 showing an even later stage in the illustrative use of the invention that is shown in part in FIG. 4.

25 FIG. 7 is a view similar to FIG. 1 showing a still later stage in the illustrative use of the invention that is shown in part in FIG. 6.

FIG. 8 is a view similar to a portion of FIG. 7 showing an even later stage in the illustrative 30 use of the invention that is shown in part in FIG. 7.

FIG. 9 is a view similar to FIG. 8 showing a still later stage in the illustrative use of the invention that is shown in part in FIG. 8.

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FIG. 10 is a view similar to FIG. 9 showing an even later stage in the illustrative use of the invention that is shown in part in FIG. 9.

5 FIG. 11 is a view similar to FIG. 10 showing a still later stage in the illustrative use of the invention that is shown in part in FIG. 10.

FIG. 12 is a view similar to FIG. 7 showing an alternative to what is shown in FIG. 7 in accordance with the invention.

10 FIG. 13 is a view similar to FIG. 8 for the alternative illustrated by FIG. 12.

FIG. 14 shows an illustrative embodiment of a portion of the FIG. 2 apparatus in more detail.

15 FIG. 15 is a view similar to FIG. 14 showing another operating condition of the FIG. 14 apparatus.

Detailed Description of the Preferred Embodiments

Although the invention is equally applicable to other medical treatments in which a portion of a patient's tubular body conduit is relocated, the 20 invention will be fully understood from the following explanation of its application to relocating a portion of a patient's internal mammary artery to provide a bypass around a narrowing in one of the patient's coronary arteries.

25 FIG. 1 shows a portion of a patient's circulatory system. The depicted portion includes aorta 10, coronary artery 20, brachiocephalic artery 12, right internal mammary artery 14, left common carotid artery 16, left subclavian artery 30, 30 and left internal mammary artery 40. Although a particular coronary artery 20 and a particular internal mammary artery 40 are employed in the illustrative procedure shown and described in detail herein, it will

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be understood that the invention is equally applicable to other coronary arteries and/or to the other internal mammary artery (i.e., the right internal mammary artery 14). Thus for convenience and in the interest 5 of generality, artery 40 will usually be referred to simply as an internal mammary artery.

FIG. 1 shows a narrowing 22 in coronary artery 20. To relieve the patient of the problems caused by narrowing 22, internal mammary artery 40 is 10 to be partly re-routed and connected to coronary artery 20 downstream from narrowing 22. In accordance with the present invention, as much as possible of the re-routing and re-connecting of artery 40 is done intralumenally (i.e., through the lumens of the 15 patient's circulatory system). This avoids or reduces the need to make incisions in the patient to gain access to the patient's interior.

As shown in FIG. 2, an illustrative procedure in accordance with this invention begins by inserting a 20 hollow tubular instrument 100 intralumenally into the patient until a distal end of instrument 100 is inside artery 30 upstream from mammary artery 40. For example, the entry point for instrument 100 may be a femoral (leg) artery of the patient, a brachial artery 25 of the patient, or any other suitable entry point which is generally remote from the site at which the bypass is to be performed. The distal portions of instrument 100 and other instruments used with instrument 100 are remotely controlled from proximal portions of those 30 instruments which remain outside the patient's body at all times. Instrument 100 is a catheter-like instrument, and any conventional catheter introducing, guiding, and/or steering technology can be used to introduce instrument 100 into the patient's circulatory

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system and cause its distal portion to ultimately pass into and along the patient's aorta to the depicted location in artery 30.

- To help temporarily anchor the distal portion 5 of instrument 100 at the depicted location in artery 30 and for other purposes to be described, an annular balloon 110 around the distal portion of instrument 100 may be inflated as shown in FIG. 2 to brace the instrument against the interior wall of artery 30.
- 10 Balloon 110 may be a perfusion balloon to allow some blood to flow past the balloon, or balloon 110 may be an occlusion balloon to substantially stop the flow of blood through artery 30. In the most preferred embodiment balloon 110 is selectively switchable
- 15 between perfusion and occlusion so that perfusion can be allowed except for relatively brief periods during which occlusion is required.

- After instrument 100 has been positioned as shown in FIG. 2, the distal portion of another 20 elongated instrument 200 is extended distally from the distal end of instrument 100 into mammary artery 40 as is also shown in FIG. 2. Instrument 200 is another catheter-like instrument which may extend coaxially through the interior of instrument 100. Instrument 200 25 is axially movable relative to instrument 100. Any conventional catheter guiding and/or steering technology may be used to get the distal portion of instrument 200 from the distal end of instrument 100 to the desired location in mammary artery 40. An annular 30 occlusion balloon 210 on the distal portion of instrument 200 may be inflated at any desired time to temporarily stop the flow of blood along artery 40 and to help anchor the distal portion of instrument 200 in that artery.

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After instrument 200 has been positioned in artery 40 as described above, the distal portion of a third elongated instrument 300 is extended distally from the distal end of instrument 200 as shown in

5 FIG. 2. The distal end of instrument 300 carries a removable, radially expandable plug 310. For example, plug 310 may be constructed generally as shown and described in Goldsteen et al. U.S. patent application No. 08/839,198, filed April 23, 1997 (Docket No.

10 293/004), which is hereby incorporated by reference herein. Instrument 300 may also be similar to the plug-deploying instrumentation shown in the immediately above-mentioned Goldsteen et al. reference. Thus instrument 300 is capable of selectively releasing plug

15 310 so that the plug radially expands to fill and occlude artery 40 downstream from the distal end of the instrumentation as shown in FIG. 3. An illustrative embodiment of plug 310 and plug-deploying apparatus 300 is shown in more detail in FIGS. 14 and 15 and

20 described in a later portion of this specification.

The next step in the illustrative procedure being described is to proximally withdraw plug-deploying instrument 300 and substitute cutting instrument 400. The distal portion of cutting instrument 400 has one or more cutting blades 410 that resiliently extend radially out from the longitudinal axis of instrument 400 when the distal portion of instrument 400 is extended distally beyond the distal end of instrument 200 as shown in FIG. 3. When blades

25 410 extend radially out, they cut through artery 40. Instrument 400 is then rotated about its longitudinal axis so that blades 410 cut through artery 40 all the way around its circumference. The upstream portion of

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artery 40 is thereby severed from the plugged downstream portion of that artery.

The next step in the illustrative procedure being described is to remove cutting instrument 400 and 5 replace it with cutting and cauterizing instrument 500 as shown in FIG. 4. Cutting and cauterizing instrument 500 includes two principal parts. These are rams-horn guide structure 510 and cutting and cauterizing structure 520. Structure 510 is inside structure 520, 10 and these two structures are axially movable relative to one another.

The distal portion of structure 510 includes resilient rams-horn-shaped guide members 512 that are resiliently biased to project radially out from and 15 then backwardly along the longitudinal axis of structure 510 outside artery 40 when the distal portion of structure 510 is extended distally beyond the distal end of instrument 200 as shown in FIG. 4.

The distal portion of structure 520 includes 20 an annular structure 522 that is resiliently biased to radially expand when pushed distally beyond the distal end of instrument 200. Structure 522 can additionally be guided by members 512 to invert and move back along the outside of artery 40 as structure 520 is pushed 25 distally relative to structure 510. For example, structure 522 may be made of a tubular braid of nitinol wires of the general type used for the frameworks of the artificial grafts shown and described in such references as Goldsteen et al. U.S. patent application 30 No. 08/745,618, filed November 7, 1996, and Bachinski et al. U.S. patent application No. 08/839,080, filed April 23, 1997 (Docket No. 293/005), both of which are hereby incorporated by reference herein. (Such a braid may also be used in plug 310.) As described in all of

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the above-mentioned references, braids or other similar structures of nitinol can be made extremely flexible and elastic so that structure 522 can have a relatively small diameter inside instrument 200, but when pushed 5 axially beyond the distal end of instrument 200, structure 522 greatly enlarges and can be made to invert and turn back on itself, all as shown in FIG. 4.

The extreme distal tip 524 of structure 522 is made cutting and cauterizing. For example, tip 524 10 may be heated electrically so that it burns through and cauterizes any tissue that connects mammary artery 40 to surrounding body structures. Structure 522 is pushed distally far enough so that tip 524 moves back up along the outside of artery 40 by a sufficient 15 distance to free the desired length of artery 40 from tissue connections to other body structures. For example, several inches of the length of severed mammary artery 40 may thus be freed from connections to other body structures.

20 As an alternative to intralumenally cutting and cauterizing tissue connections to severed mammary artery 40, this may be done through a trocar or other similar instrument inserted through the patient's chest wall. This alternative is illustrated by FIG. 5, which 25 shows trocar tube 600 being used to introduce tissue cutting instrument 610 and tissue cauterizing instrument 620 into the patient to cut and cauterize tissue connections to severed mammary artery 40.

The next step in the illustrative procedure 30 being described is to proximally withdraw instrumentation 500 (assuming that instrumentation 500 was used). It may then be desirable to somewhat proximally retract instrument 200 as shown in FIG. 6. To do this, occlusion balloon 210 is deflated, and

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after instrument 200 has been suitably retracted, a second occlusion balloon 220 (which is closer than balloon 210 to the distal end of instrument 200) is inflated. During this phase of the procedure
5 balloon 110 preferably occludes artery 30.

The next step is to insert steerable video instrumentation 700 into the patient as shown in FIG. 6. Steerable video instrumentation 700 may be similar to the steerable video instrumentation shown
10 and described in any of Goldsteen et al. U.S. patent application No. 08/745,618, filed November 7, 1996, Bachinski et al. U.S. patent application No. 08/842,391, filed April 23, 1997 (Docket No. 293/006), and Sullivan et al. U.S. patent application
15 No. 08/844,992, filed April 23, 1997 (Docket No. 293/007), all of which are hereby incorporated by reference herein. Thus instrumentation 700 typically includes a light source for illuminating the interior
20 of the patient beyond the distal end of instrumentation 700. Instrumentation 700 also typically includes video components for capturing an image of the interior of the patient beyond the distal end of the instrumentation and for transmitting that image back to a video display which is outside the patient.
25 Instrumentation 700 still further includes steering components that can be controlled from outside the patient to cause the distal portion of the instrumentation to curve and otherwise deflect laterally. And instrumentation 700 may include an
30 axially reciprocable longitudinal member 750 for making an initial penetration of the side wall of coronary artery 20 after other components of the instrumentation have been used to position the distal portion of instrumentation 700 adjacent the coronary artery.

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FIG. 7 shows the condition of the patient after the distal portion of instrumentation 700 has been steered to a location adjacent coronary artery 20 downstream from narrowing 22, and also after 5 longitudinal member 750 has been extended from the distal end of instrumentation 700 through the side wall of the coronary artery and into the lumen of that artery. It should be noted that instrumentation 700 takes with it the severed portion of mammary artery 40 10 as instrumentation 700 is steered to coronary artery 20. Thus the severed end of the upstream portion of mammary artery 40 is also adjacent coronary artery 20 in FIG. 7. Longitudinal member 750 may be a sharply pointed wire that is capable of being pushed through 15 the wall of coronary artery 20 and down into the lumen of the coronary artery. After member 750 has been pushed down into the lumen of coronary artery 20, it helps to keep the severed end of mammary artery 40 adjacent the coronary artery as shown in FIG. 7.

20 The next step in the illustrative procedure being described is to proximally withdraw instrumentation 700, except for longitudinal member 750. Then connector instrumentation 800 is inserted 25 into the patient through instrument 200 and concentrically around longitudinal member 750 as shown in FIG. 8.

Connector instrumentation 800 includes an inner tubular member 810 concentrically surrounded by an outer tubular member 820. Inside the distal portion 30 of outer tubular member 820 is a connector structure 830. Connector structure 830 includes a serpentine ring 832. Struts 834 extend distally from the distal peaks of the convolutions of ring 832. Struts 834 are bound into a cone shape by annular band 836. An

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annular elastic web 838 (e.g., of silicone) is preferably provided between struts 834.

The first step in the use of instrumentation 800 is to push connector structure 830 distally out of 5 the distal end of tubular member 820 as shown in FIG. 9. This may be done by somewhat inflating annular balloon 812 on the distal portion of tubular member 810 and pushing members 810 and 812 distally relative to member 820. When connector structure 830 is beyond the 10 distal end of member 820, ring 820 expands elastically by itself (or is expanded plastically by further inflation of balloon 812 inside ring 832) to firmly annularly engage the inner surface of the distal portion of mammary artery 40.

15 The next step is to force the cone of struts 834 and the associated web 838 to follow longitudinal member 750 through the side wall of coronary artery 20 as shown in FIG. 10. Any or all of elements 810, 812, and 820 can be pushed distally to push elements 834 and 20 838 through the coronary artery wall, gradually enlarging the initial aperture previously made by longitudinal member 750 as elements 834 and 838 enter that aperture.

When struts 834 and web 838 are through the 25 side wall of coronary artery 20 to the desired degree, balloon 812 is further inflated inside the cone of struts 834. This causes band 836 to break or otherwise cease to hold struts 834 in their initial cone shape. When released from band 836, struts 834 flare radially 30 out inside coronary artery 20 as they are resiliently biased to do (see FIG. 11). Web 838 continues to provide an annular structure between the struts. In the condition shown in FIG. 11 connector 830 provides a permanent tubular connection between the severed end of

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mammary artery 40 and the side wall of coronary artery 20. When all of the instrumentation other than connector 830 is proximally withdrawn from the patient, blood flows through mammary artery 40 and connector 830 5 into coronary artery 20 downstream from narrowing 22. This provides the desired bypass around narrowing 22 and concludes the illustrative procedure being described.

A possible modification of the above-10 described procedure is shown beginning with FIG. 12. In this alternative another catheter-type instrument 900 is inserted into the patient's circulatory system so that a distal portion of that instrument extends from aorta 10 into coronary artery 20 through narrowing 15 22 to the point at which it is desired to connect the severed end of mammary artery 40. Insertion of instrument 900 can be done at any time relative to insertion and use of the other instrumentation described above. Instrument 900 can serve as a source 20 of radiologic fluid in coronary artery 20. Alternatively or additionally, instrument 900 can include radiologic markers in the coronary artery region. These possible radiologic uses of instrument 900 can help the physician make the proper approach to 25 the coronary artery with the severed end of mammary artery 40. As still another possibility, instrument 900 can provide a source of light in coronary artery 20 to help the physician, using the video features of instrumentation 700, make the proper 30 approach with the severed end of mammary artery 40 to the coronary artery.

Instrument 900 may include a longitudinal member 910 which may be somewhat like above-described member 750. At any suitable time after instrument 900

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is properly positioned in coronary artery 20, the distal portion of member 910 may be pushed out through the coronary artery wall as shown in FIG. 12. Member 910 may then be used in any of several ways. For 5 example, the distal end of member 910 may provide a light source or another type of highly visible target for facilitating proper relocation of the severed end of mammary artery 40 using the video components of instrument 700. Alternatively or additionally, 10 instrument 700 may include a snare 750a (e.g., at the distal end of longitudinal member 750) for engaging the distal portion of member 910 outside the coronary artery. In that case, after member 910 has been snared, member 750 may be proximally withdrawn while 15 more of member 910 is fed into the patient until member 910 forms one continuous structure at least between arteries 20 and 40, and more preferably into the patient via instrument 900, out the wall of coronary artery 20, into the severed end of mammary artery 40, 20 and out of the patient via instrument 700. Used in this way, member 910 provides a very stable structure for maintaining mammary artery 40 in its desired new location and for guiding connector instrumentation 800 to the location at which connector structure 830 must 25 be installed between the severed end of the mammary artery and the side wall of the coronary artery.

FIG. 13 shows how FIG. 8 is modified for the alternative of FIG. 12, the only difference between FIGS. 8 and 13 being that member 910 replaces member 30 750. The exact same modification is all that is required to adapt FIGS. 9-11 for this alternative procedure. Providing one continuous structure like member 910 into the patient, through an operative site, and then out of the patient again is similar to what is

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done in above-mentioned Goldsteen et al. application No. 08/745,618, and additional details regarding this type of technique and instrumentation suitable for implementing this type of technique will be found in 5 that reference, and also in Bachinski et al. U.S. patent application No. 08/842,391, filed April 23, 1997 (Docket No. 293/006), and Bachinski et al. U.S. patent application No. 08/844,910, filed April 23, 1997 (Docket No. 293/010), all of which are hereby 10 incorporated by reference herein.

Connector structure 830 is only one example of many types of connectors that may be used. For example, in addition to the structure shown in FIGS. 8-11 and 13, connector structure 830 may have prongs that 15 extend radially out from ring 832 and that can enter the tissue of mammary artery 40 to help secure the connector to that artery. Connector structure 830 may also have hooks and/or barbs on the distal ends of struts 834 to help the struts better and more securely 20 engage coronary artery 20 when struts 834 are deployed as shown in FIG. 11. Examples of suitable materials for connector structure 830 are nitinol or stainless steel for all components other than web 838, and silicone for web 838. Additional information regarding 25 possible connector structures and instrumentation for delivering and deploying such structures will be found in above-mentioned Goldsteen et al. application No. 08/745,618, and also in Sullivan et al. U.S. patent application No. 08/844,992, filed April 23, 1997 (Docket No. 293/007), and Bachinski et al. U.S. patent application No. 08/839,199, filed April 23, 1997 (Docket No. 293/008), all of which are hereby 30 incorporated by reference herein.

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FIGS. 14 and 15 show an illustrative embodiment of elements 300 and 310 in more detail. In this embodiment plug 310 has the shape of a tube with a closed end (toward the right in FIGS. 14 and 15). Plug 5 310 is made from an elastic mesh framework 320 covered with an elastic covering 330 which substantially fills the apertures in the mesh. For example, framework 320 may be a braid of nitinol wires, and covering 330 may be a web of silicone. Plug 310 is made so that its 10 substantially relaxed state is as shown in FIG. 15. In this substantially relaxed condition plug 310 has a relatively large diameter (the vertical dimension as viewed in FIG. 15) and a relatively short length (the horizontal dimension as viewed in FIG. 15). However, 15 plug 310 can be elastically deformed to the size and shape shown in FIG. 14 by stretching it axially over the outside of tubular member 300. When thus stretched, the length of the tube increases substantially, but its diameter decreases. In 20 addition, part of the material in its closed end is deformed into more tubular length. After stretching over tube 300, plug 310 is releasably held in that condition by a loop of wire 340 which passes out through aperture 350 in the side wall of tube 300 and 25 through a portion of the side wall of the tubular part of the plug as shown in FIG. 14.

In use, plug 310 is inserted into the patient (FIG. 2) in the condition shown in FIG. 14. When the plug is properly positioned in the patient and it is 30 desired to release the plug, the tension on wire loop 340 is relaxed. This allows plug 310 to begin to return to a shape more like its relaxed shape. In particular, plug 310 begins to axially shorten and to increase in diameter. When it is desired to completely

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release plug 310 from the apparatus, one tail of wire loop 340 is released and the other tail of the loop is pulled proximally out of the patient. Eventually the released tail is pulled completely out of plug 310 as 5 shown in FIG. 15 and the plug is thereby completely released from the apparatus.

As has been said, although the shape of plug 310 may be somewhat different from the plug shapes shown in above-mentioned Goldsteen et al. application 10 No. 08/839,198 (Docket No. 293/004), plug 310 may in other respects be constructed as shown and described in that reference.

It will be understood that the foregoing is only illustrative of the principles of the invention, 15 and that various modifications can be made by those skilled in the art without departing from the scope and spirit of the invention. For example, the depicted connector structure 830 is only one example of many connector structures that can be used, other examples 20 being shown and described in several of the references that are mentioned above. Similarly, the particular internal mammary bypass procedure shown and described herein is only one example of medical treatments to which the invention or various aspects of the invention 25 can be applied. For example, the invention is equally applicable to relocating and reconnecting other portions of a patient's circulatory system tubing or other non-circulatory system tubing of a patient. Radiologic markers can be provided at any desired 30 locations on any of the instrumentation of the invention to help the physician radiologically monitor instrumentation positions within the patient. Alternatively or in addition, any of the instrumentation of the invention can be used to

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introduce radiologic fluids into the patient to facilitate radiologic monitoring of the procedure.

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The Invention Claimed Is

1. A method for relocating a patient's tubular body conduit comprising:
 - inserting instrumentation into and axially along the conduit;
 - using the instrumentation to make an annular cut in the conduit;
 - using the instrumentation to shift the cut end of the conduit to a new location in the patient's body; and
 - connecting the cut end of the conduit to the patient's body at the new location.
2. The method defined in claim 1 wherein the new location is adjacent another tubular body conduit, and wherein the connecting comprises:
 - making a tubular connection between the cut end and the other conduit.
3. The method defined in claim 2 wherein the new location is adjacent a side wall of the other conduit and wherein the making comprises:
 - forming an aperture in the side wall;
 - and
 - attaching the cut end to the other conduit via the aperture.
4. The method defined in claim 1 wherein the connecting comprises:
 - using the instrumentation to deliver a connector to the cut end.

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5. The method defined in claim 4 wherein the connecting further comprises:

using the instrumentation to install the connector at the cut end.

6. The method defined in claim 3 wherein the attaching comprises:

using the instrumentation to deliver a connector to the cut end.

7. The method defined in claim 6 wherein the attaching further comprises:

using the instrumentation to install the connector between the cut end and the other conduit via the aperture.

8. The method defined in claim 1 further comprising:

using the instrumentation to install a plug in the conduit at a location spaced from the location at which the annular cut will be made in the conduit.

9. The method defined in claim 1 further comprising:

cutting tissue outside the conduit that connects the conduit to other body structure of the patient.

10. The method defined in claim 9 further comprising:

cauterizing tissue cut in the cutting.

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11. The method defined in claim 1 further comprising:

extending a portion of the instrument from the cut end and back along the outside of the conduit to cut tissue outside the conduit that connects the conduit to other body structure of the patient.

12. The method defined in claim 11 further comprising:

cauterizing the tissue cut in the extending.

13. The method defined in claim 1 wherein the conduit is an internal mammary artery of the patient.

14. The method defined in claim 2 wherein the conduit is an internal mammary artery of the patient and wherein the other conduit is a coronary artery of the patient.

15. Apparatus for installing a plug in a lumen of a body conduit comprising:

a longitudinal structure configured for insertion into and along the lumen, the longitudinal structure being adapted to releasably carry a plug structure and to releasably retain the plug structure in a configuration small enough to pass along the lumen with the longitudinal structure, and the longitudinal structure including a plug releasing substructure configured to selectively release the plug structure from the longitudinal structure so that the plug structure can enlarge to plug the lumen.

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16. The apparatus defined in claim 15
wherein the plug structure comprises:
an elastic framework; and
an elastic covering over the framework.

17. The apparatus defined in claim 16
wherein the framework is resiliently biased to enlarge
to a size which will plug the conduit when the plug
structure is released from the longitudinal structure.

18. The apparatus defined in claim 17
wherein the framework defines a tube having a closed
end.

19. The apparatus defined in claim 18
wherein the tube is elastically deformable to a greater
length and smaller diameter than its relaxed length and
diameter.

20. The apparatus defined in claim 19
wherein the longitudinal structure deforms the tube to
the greater length and smaller diameter, with the
length of the tube being parallel to the longitudinal
axis of the longitudinal structure.

21. The apparatus defined in claim 20
wherein the plug releasing substructure is configured
to release the tube from the longitudinal structure so
that the tube can return to its relaxed length and
diameter with the longitudinal axis of the tube
parallel to the longitudinal axis of the lumen.

22. The apparatus defined in claim 16
wherein the framework comprises nitinol.

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23. The apparatus defined in claim 16
wherein the covering comprises silicon.

24. Apparatus for relocating a patient's
tubular body conduit comprising:

a longitudinal structure configured for
insertion into and along the lumen of the conduit, the
longitudinal structure including:

a first substructure configured to make
an annular cut in the conduit;

a second substructure configured to
shift the cut end of the conduit to a new location in
the patient's body; and

a third substructure configured to
connect the cut end of the conduit to the patient's
body at the new location.

25. The apparatus defined in claim 24
wherein the longitudinal structure further includes:

a fourth substructure configured to plug
the conduit.

26. The apparatus defined in claim 25
wherein the fourth substructure comprises:

a plug-installing structure configured
to install a plug in the lumen of the conduit.

27. The apparatus defined in claim 24
wherein the first substructure comprises:

a tissue cutter selectively extendable
radially out from the longitudinal axis of the
longitudinal structure.

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28. The apparatus defined in claim 27 wherein the first substructure further comprises:

a support structure for the tissue cutter, the support structure being rotatable about the longitudinal axis of the longitudinal structure in order to rotate the tissue cutter about the longitudinal axis and produce the annular cut in the conduit.

29. The apparatus defined in claim 24 wherein the third substructure is configured to make a tubular connection between the cut end of the conduit and another tubular body conduit at the new location.

30. The apparatus defined in claim 29 wherein the third substructure comprises:

a tubular connector configured to annularly engage the cut end of the conduit and a side wall of the other conduit via an aperture in the side wall at the new location.

31. The apparatus defined in claim 29 wherein the third substructure comprises:

a tissue penetrating structure configured to penetrate a side wall of the other conduit at the new location.

32. The apparatus defined in claim 31 wherein the third substructure further comprises:

a tubular connector disposed around the tissue penetrating structure and configured to partly follow the tissue penetrating structure through the side wall of the other conduit, thereby producing an enlarged aperture through the side wall.

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33. The apparatus defined in claim 32 wherein the third substructure further comprises:
a connector deploying structure configured to cause an axial portion of the connector to annularly engage the cut end of the conduit.

34. The apparatus defined in claim 32 wherein the third substructure further comprises:
a connector deploying structure configured to cause an axial portion of the connector to annularly engage the side wall of the other conduit inside the enlarged aperture through the side wall.

35. The apparatus defined in claim 29 further comprising:
a tissue penetrating structure extending along the lumen of the other conduit and partly out through the side wall of the other conduit at the new location.

36. The apparatus defined in claim 35 wherein the third substructure further comprises:
a structure configured to selectively couple with the part of the tissue penetrating structure which extends out through the side wall of the other conduit at the new location to produce a linking structure between the cut end and the other conduit.

37. The apparatus defined in claim 36 wherein the third substructure further comprises:
a tubular connector disposed around the linking structure and configured to partly follow the linking structure through the side wall of the other

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conduit, thereby producing an enlarged aperture through the side wall.

38. The apparatus defined in claim 37 wherein the third substructure further comprises:

a connector deploying structure configured to cause an axial portion of the connector to annularly engage the cut end of the conduit.

39. The apparatus defined in claim 37 wherein the third substructure further comprises:

a connector deploying structure configured to cause an axial portion of the connector to annularly engage the side wall of the other conduit inside the enlarged aperture through the side wall.

40. The apparatus defined in claim 24 wherein the longitudinal structure further includes:

a fourth substructure configured to selectively emerge from the cut end of the conduit and move back along the outside of the conduit to cut tissue connecting the conduit to other body structure of the patient.

41. The apparatus defined in claim 40 wherein the fourth substructure is additionally configured to cauterize cut connecting tissue.

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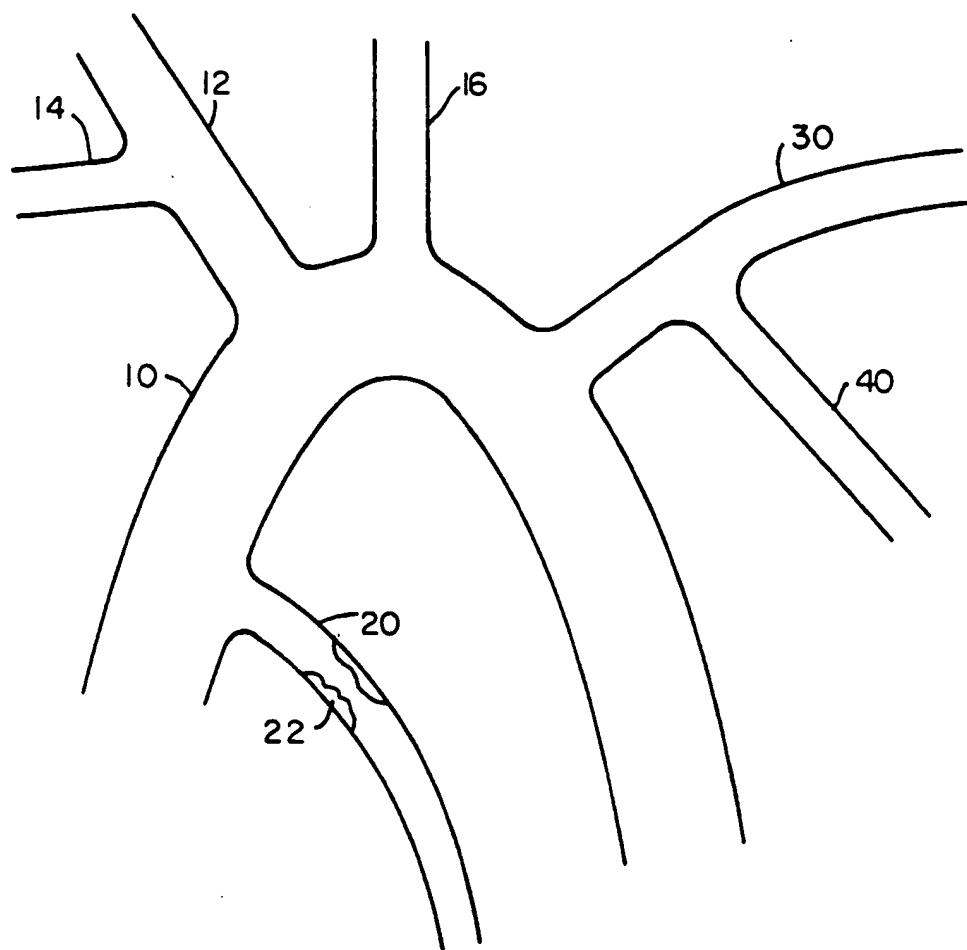
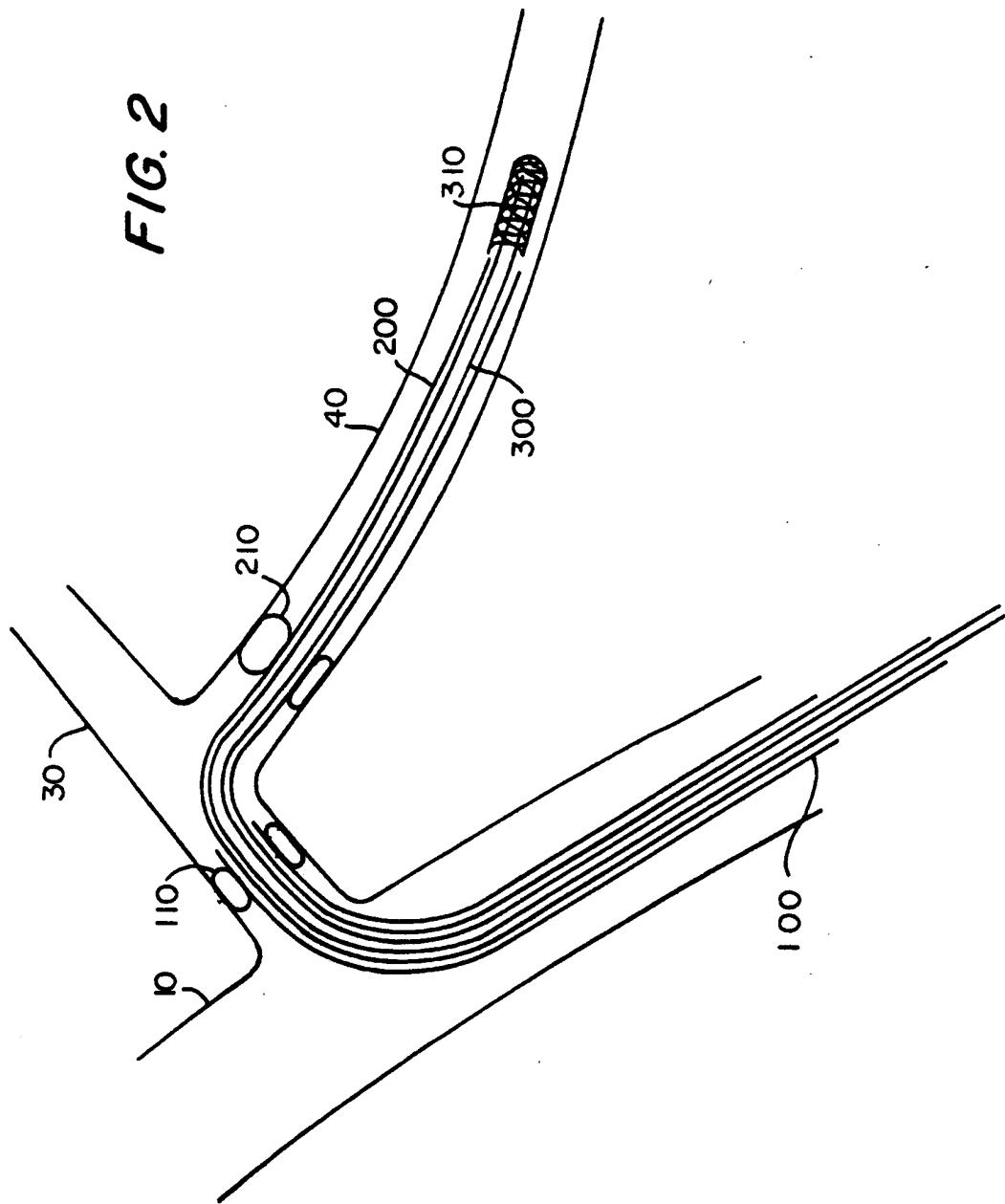


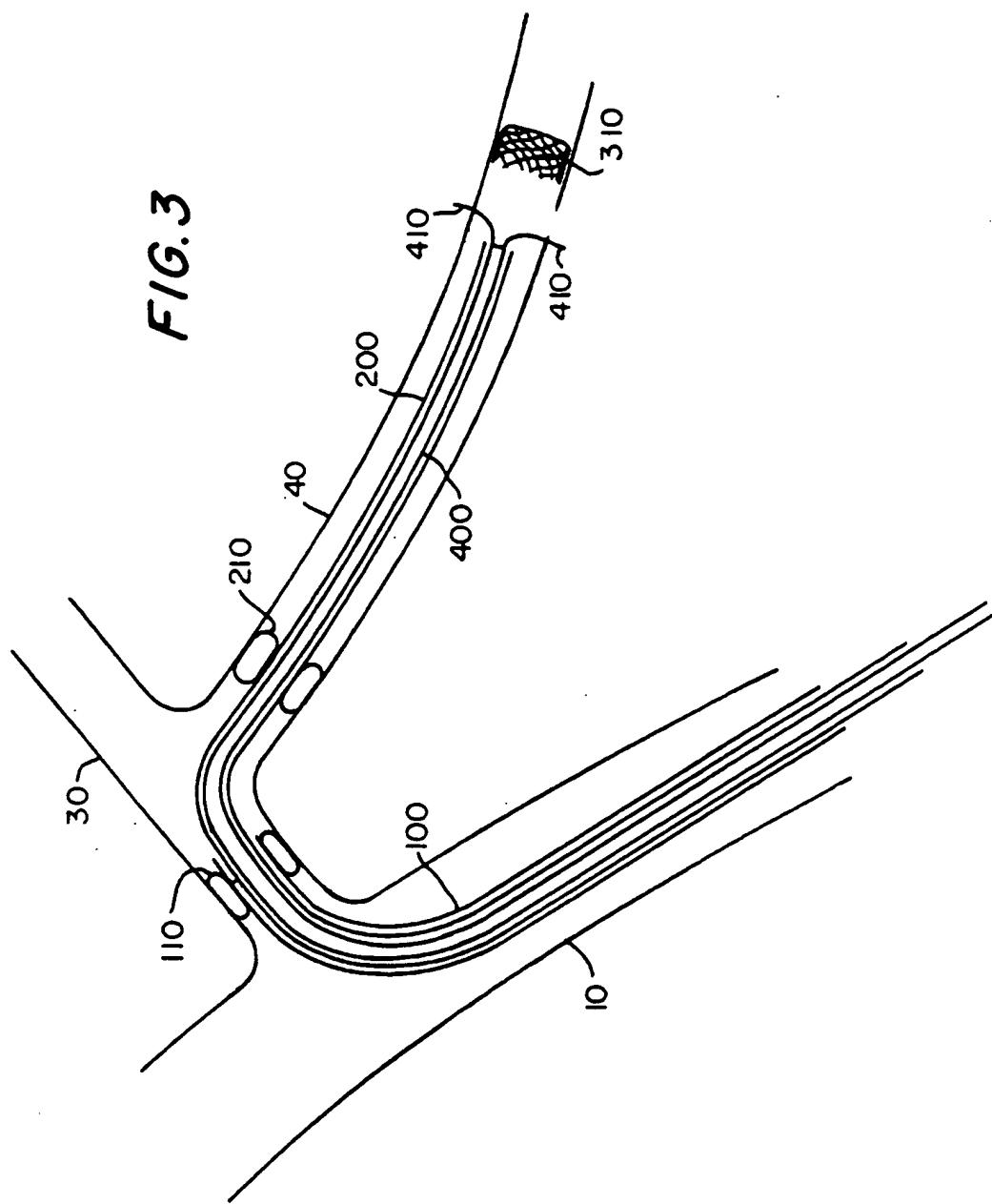
FIG. 1

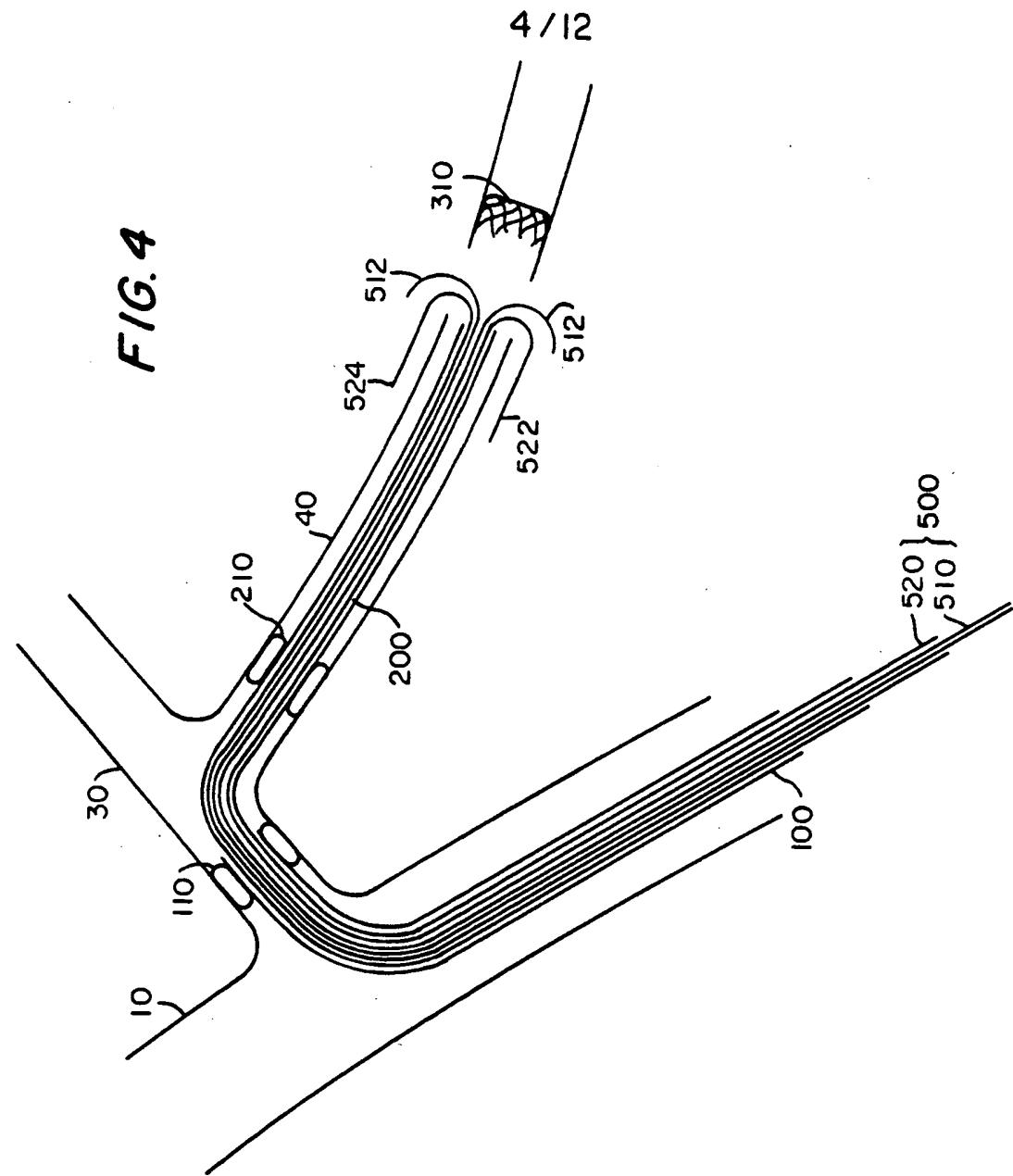
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FIG. 2



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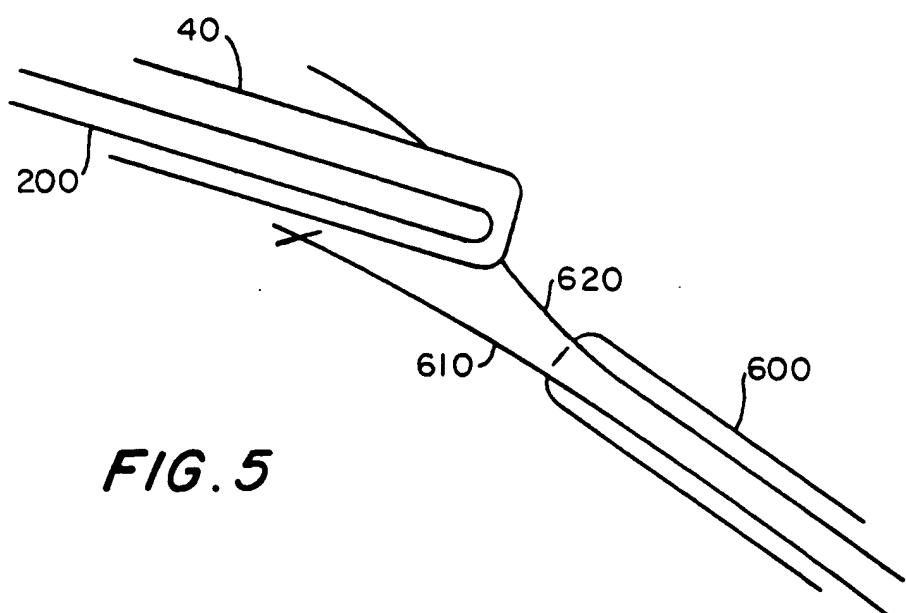
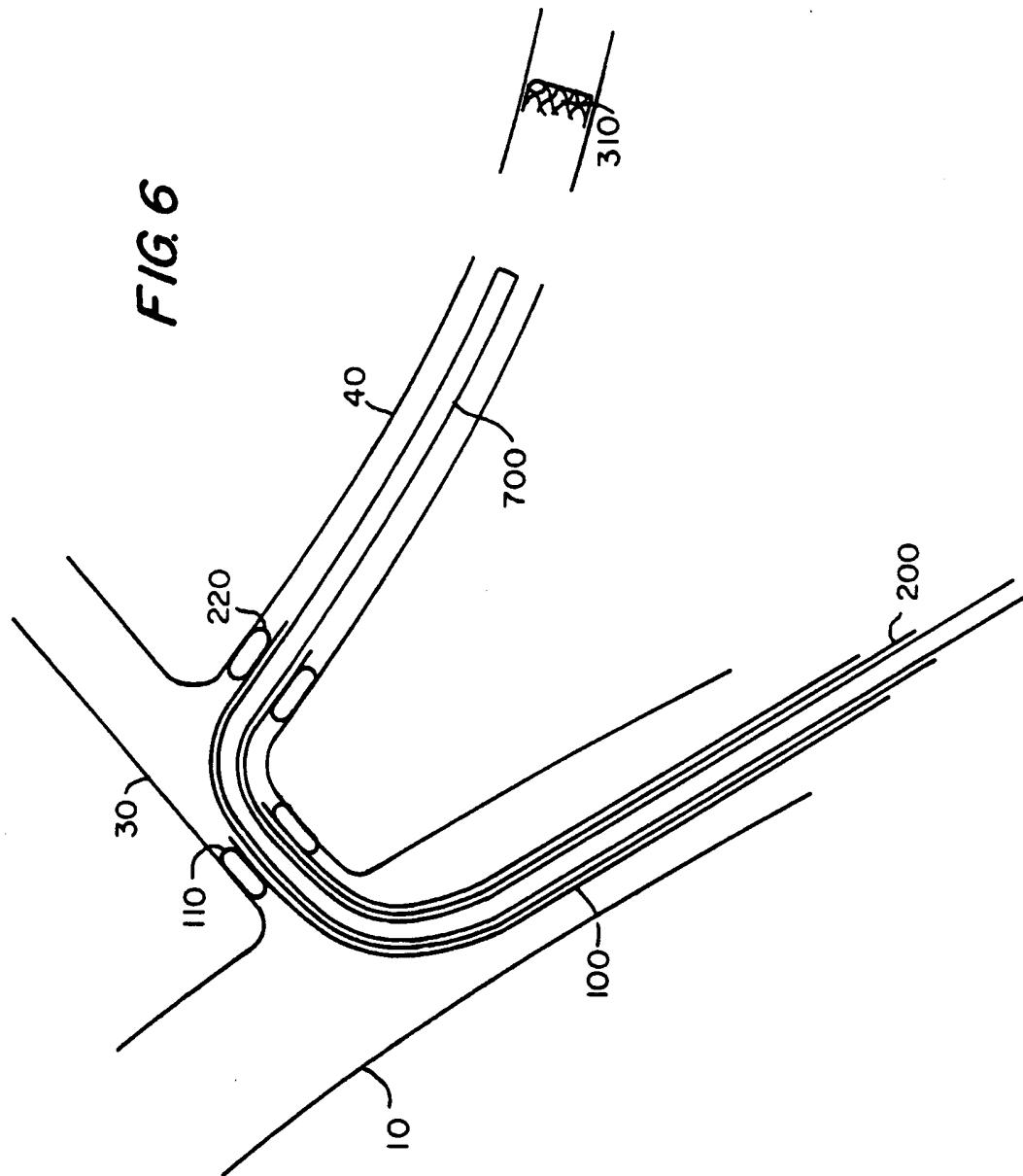


FIG. 5

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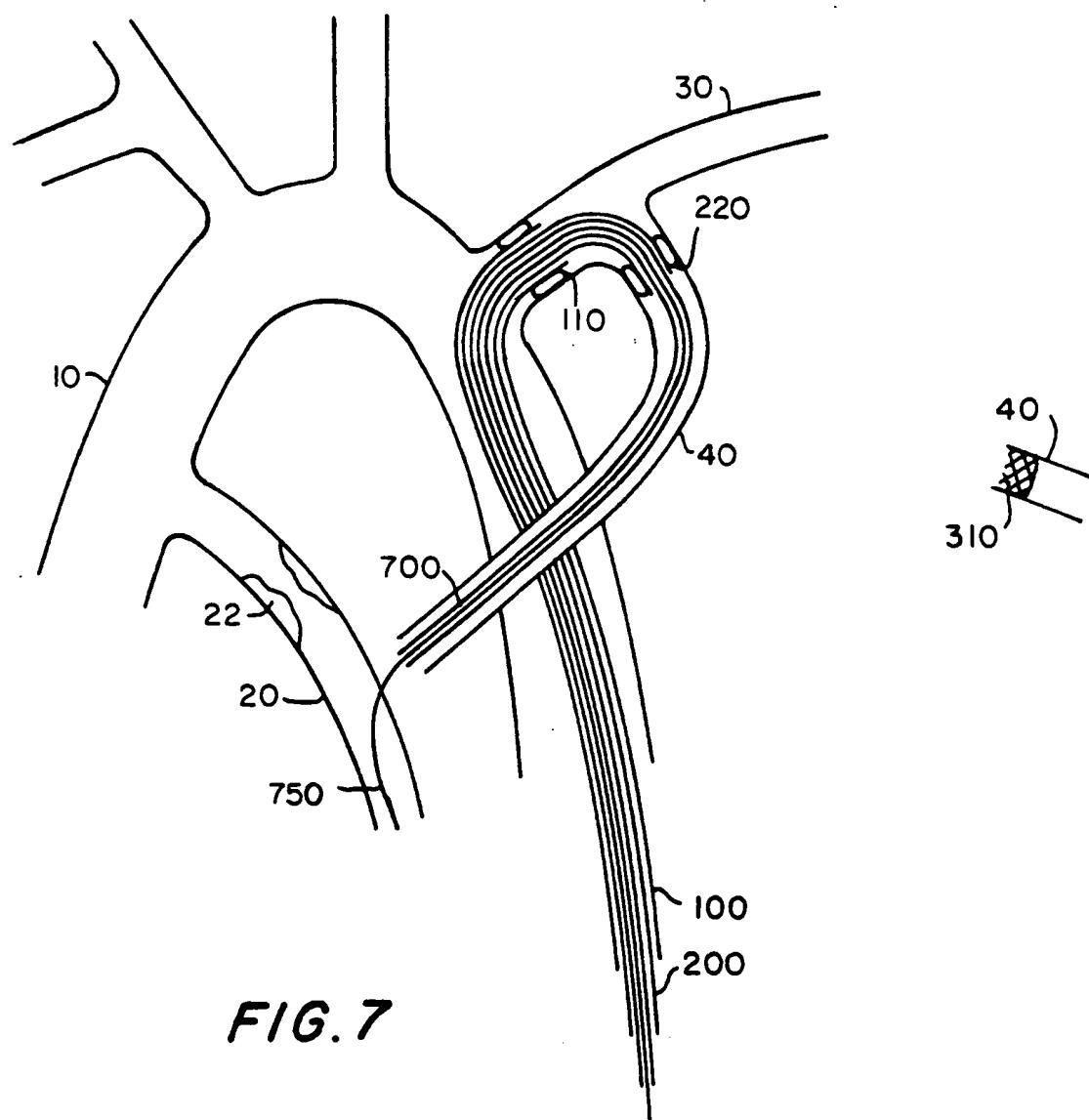


FIG. 7

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FIG. 8

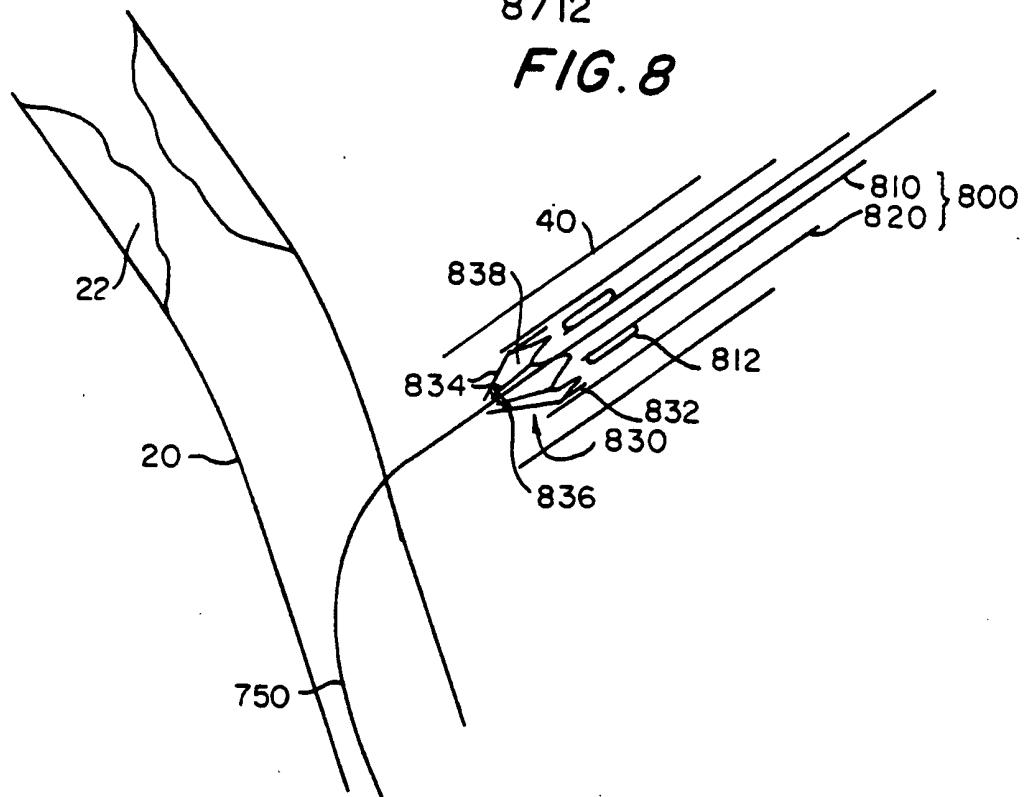
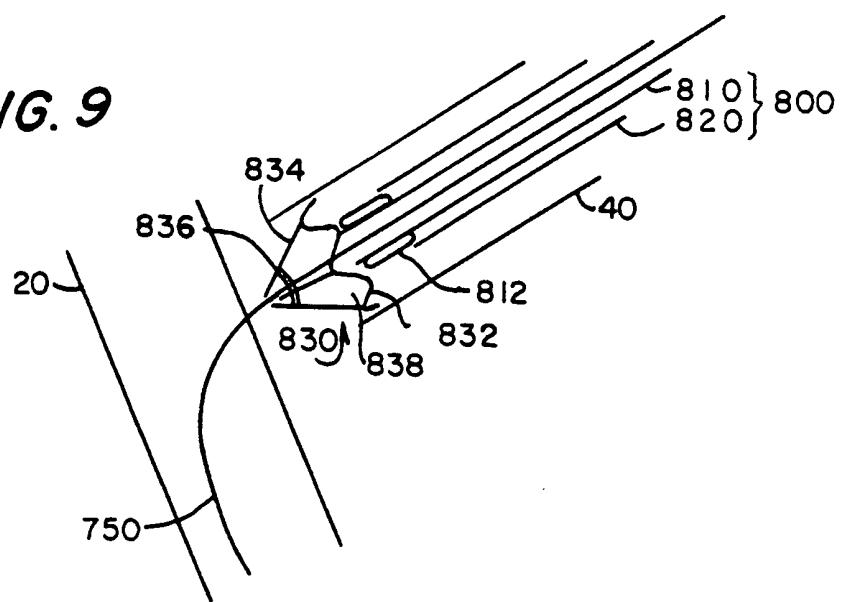


FIG. 9



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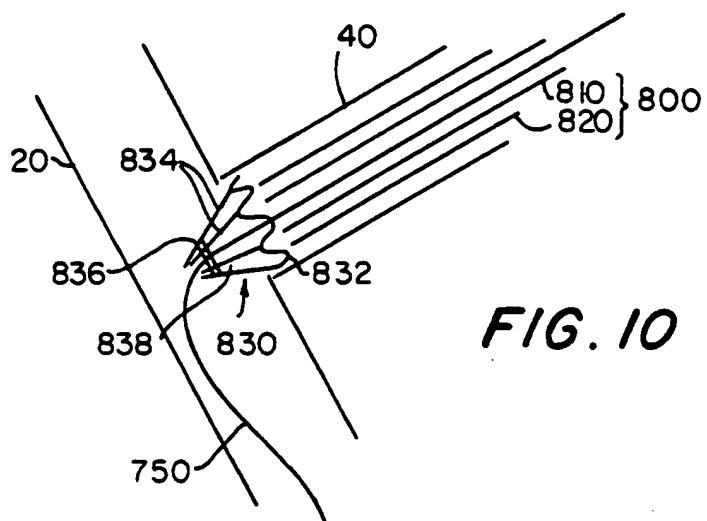


FIG. 10

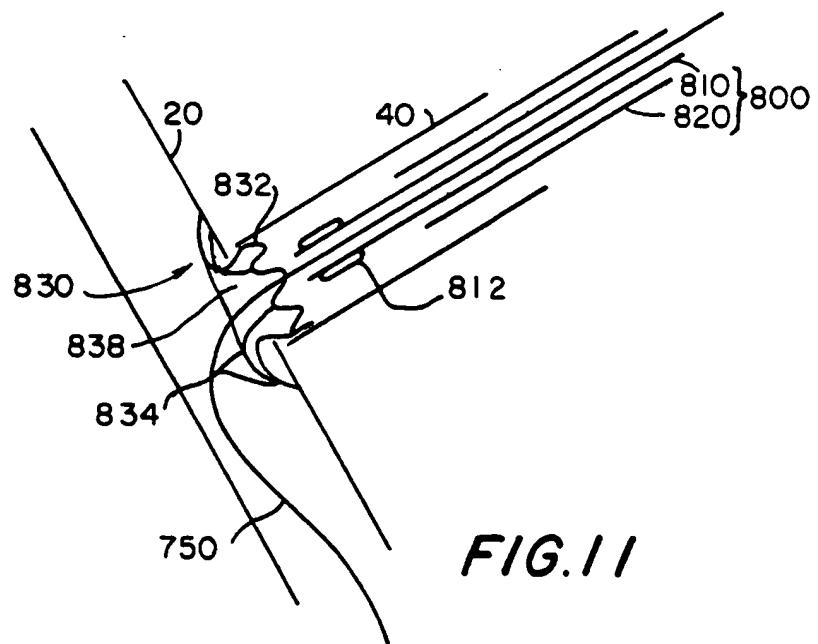


FIG. 11

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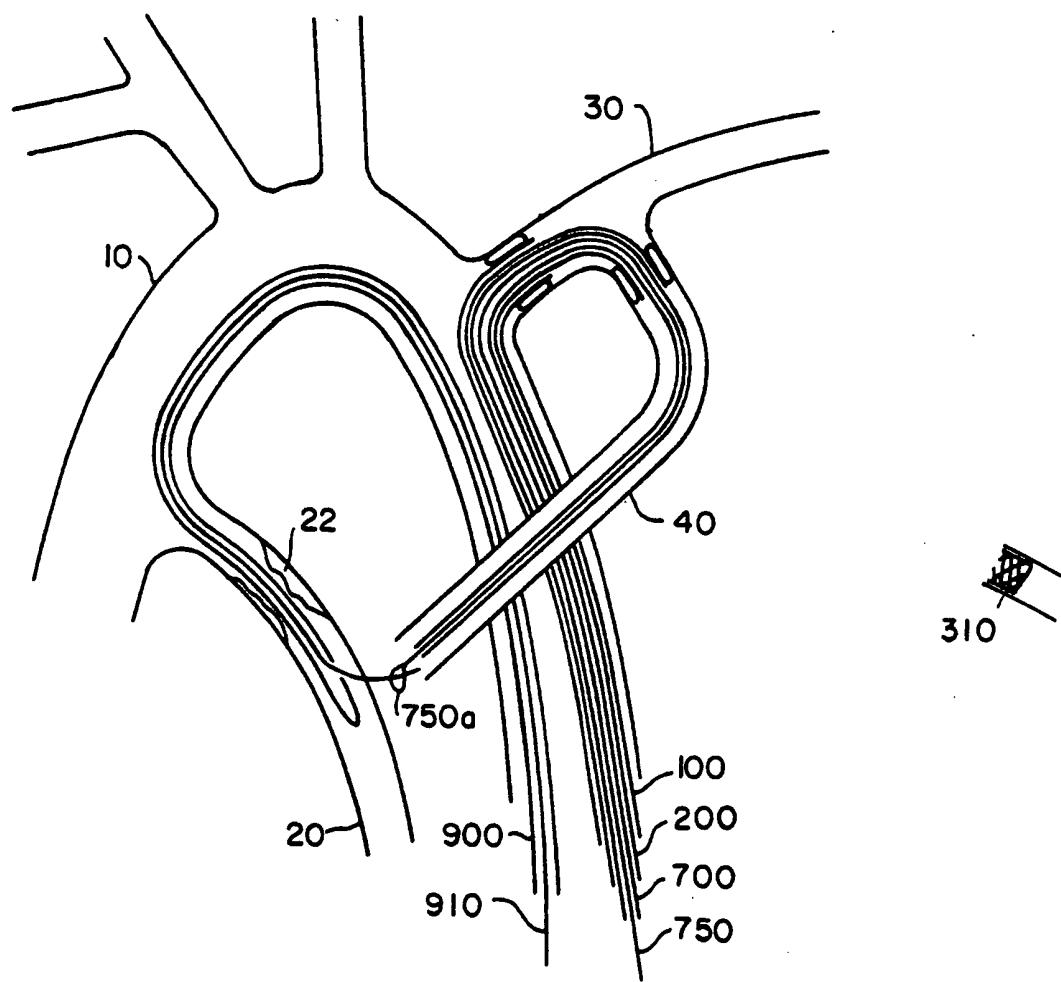
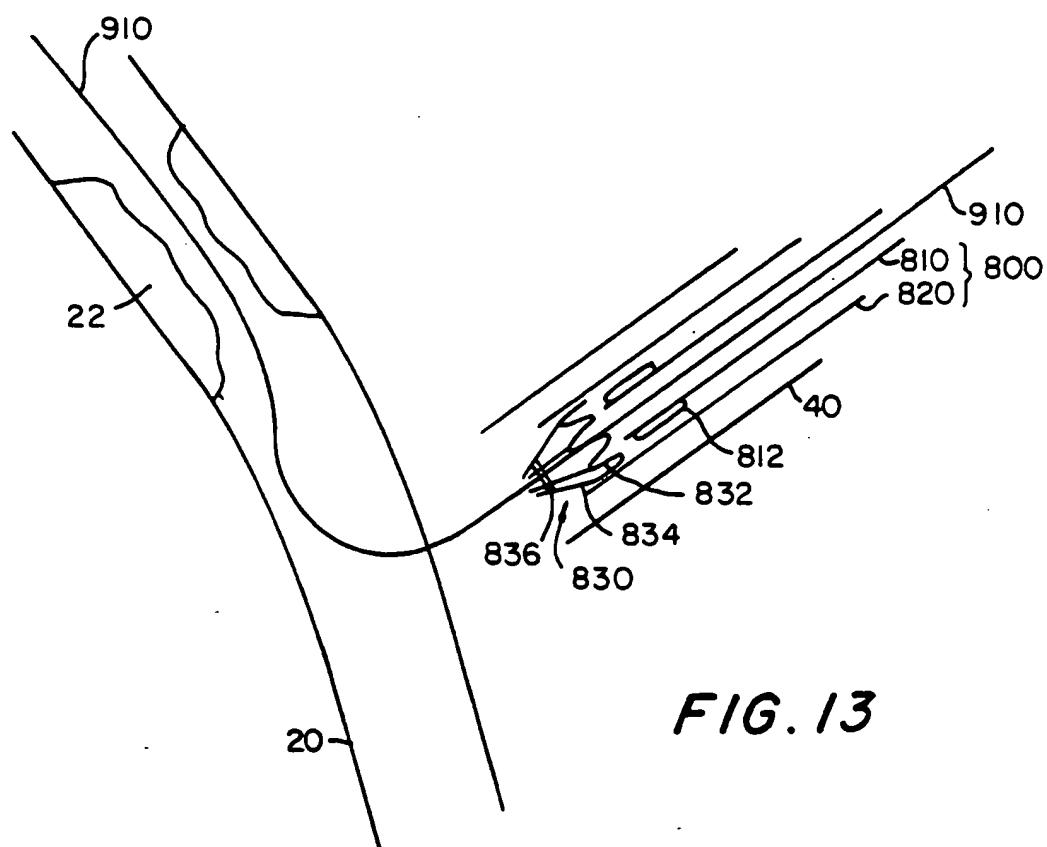


FIG. 12

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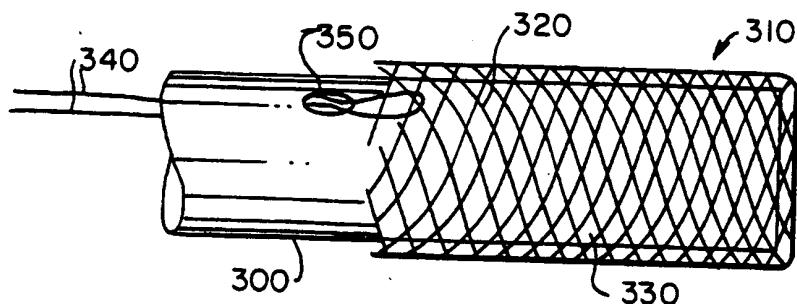


FIG. 14

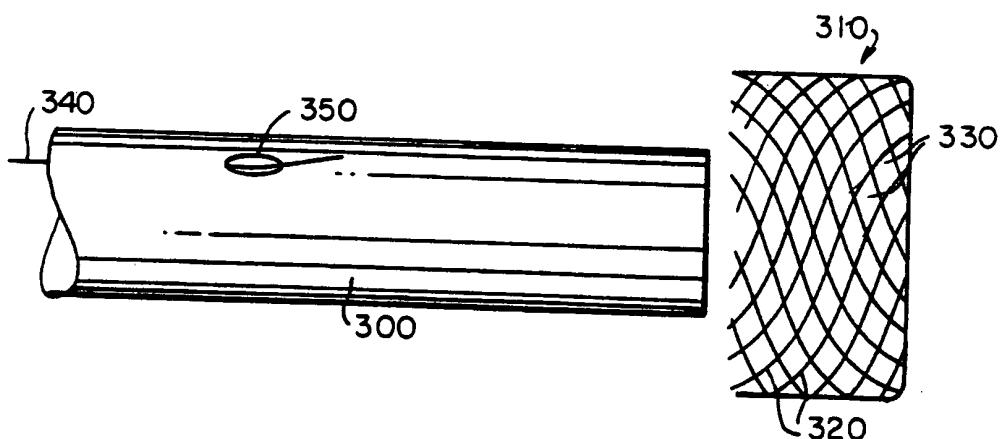


FIG. 15